

Fluid Dynamics =

flow of liquids and gases.

biological examples

- swimming and flying
- blood flow
- cytoskeleton
fluid-like on long time scales.

physics

- fluid
 - condensed matter -
 - translational + rotational invariance



- coarse-grained theory involving small number of effective degrees of freedom.

forces \longleftrightarrow flows

Assumption

- iso-thermal
- single component
- locally structureless

Counter-example

- convective flow
- vinicigarette
- lipid crystal

$\rho(x) \equiv$ local fluid density

$\underline{v}(x) \equiv$ flow field

$\underline{\underline{\sigma}}(x) \equiv$ stress tensor $[N/m^2]$

- rank 2 (3×3)

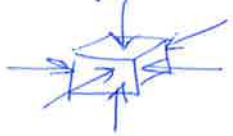
- contact forces acting on fluid element

fluid element



$\underline{\underline{\sigma}} \cdot \underline{n} =$ force density acting on boundary

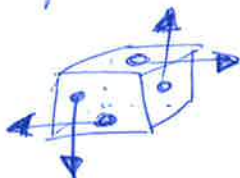
example 1:



pressure

$$\underline{\underline{\sigma}} = -p \underline{\underline{I}} = \begin{pmatrix} -p & 0 & 0 \\ 0 & -p & 0 \\ 0 & 0 & -p \end{pmatrix}$$

example 2




shear stress

$$\underline{\underline{\sigma}} = \begin{pmatrix} 0 & s & 0 \\ s & 0 & 0 \\ 0 & 0 & 0 \end{pmatrix}$$

Notation: Landau-Lifshitz \neq Happel-Biscamp

Why stress tensor symmetric?

- stress tensor = contact force
- anti-symmetric part
= external torque 
- ≠ contact force.

- external torque on fluid element would result in rigid body rotation, irrelevant for coarse-grained description of unstructured fluid.

- for structured fluids, (eg. liquid crystals), external angular momentum can be converted into internal angular momentum

The strain rate tensor characterizes "deformations" of fluid elements.

$$2 \underline{\underline{\Gamma}} = \nabla \underline{v} + (\nabla \underline{v})^T$$

$$\Gamma_{ij} = \frac{1}{2} (\partial_i v_j + \partial_j v_i)$$

- pure translation $\Gamma = 0$

- pure rotation $\Gamma = 0$

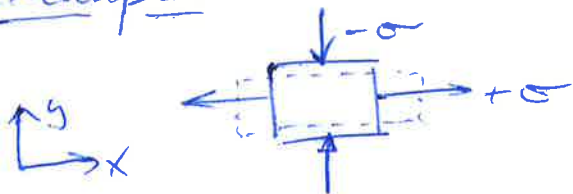
- dilation part: $\Gamma_0 = \frac{1}{3} \text{tr} \Gamma \cdot \underline{\underline{I}}$
 $\text{tr} \Gamma \equiv$ rate of volume change of fluid element

- shear

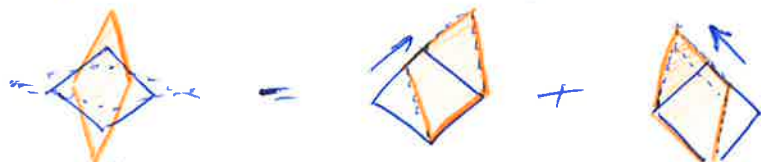
$$\Delta = \Gamma - \frac{1}{3} \text{tr} \Gamma \cdot \underline{\underline{I}}$$

\equiv shear rate tensor

examples



$$\Delta = \begin{pmatrix} \sigma & 0 & 0 \\ 0 & -\sigma & 0 \\ 0 & 0 & 0 \end{pmatrix}$$



$$\underline{\underline{\Delta}} = R_2(45^\circ) \underline{\underline{\Delta}} R_2(45^\circ) = \begin{pmatrix} 0 & -\sigma & 0 \\ -\sigma & 0 & 0 \\ 0 & 0 & 0 \end{pmatrix}$$

$$\underline{\underline{\Pi}} = -\underline{\underline{\sigma}} + \rho \underline{v} \otimes \underline{v}$$

\equiv "momentum flux tensor" (LL)

\equiv "total stress tensor" [HB]

Structure of stress tensor, $\underline{\underline{\sigma}}$
under reversal of time arrow.

$$t \rightarrow -t$$

$$\underline{v} \rightarrow -\underline{v}$$

$$p \rightarrow p$$

$$\underline{\underline{\sigma}} \rightarrow -\underline{\underline{\sigma}}$$

$$\underline{\underline{\sigma}} = \underbrace{-p \underline{\underline{I}}}_{\text{reversible part}} + \underbrace{\underline{\underline{\sigma}}'}_{\text{irreversible part}}$$

reversible part \equiv
hydrostat. pressure

irreversible part
 \equiv viscous stress

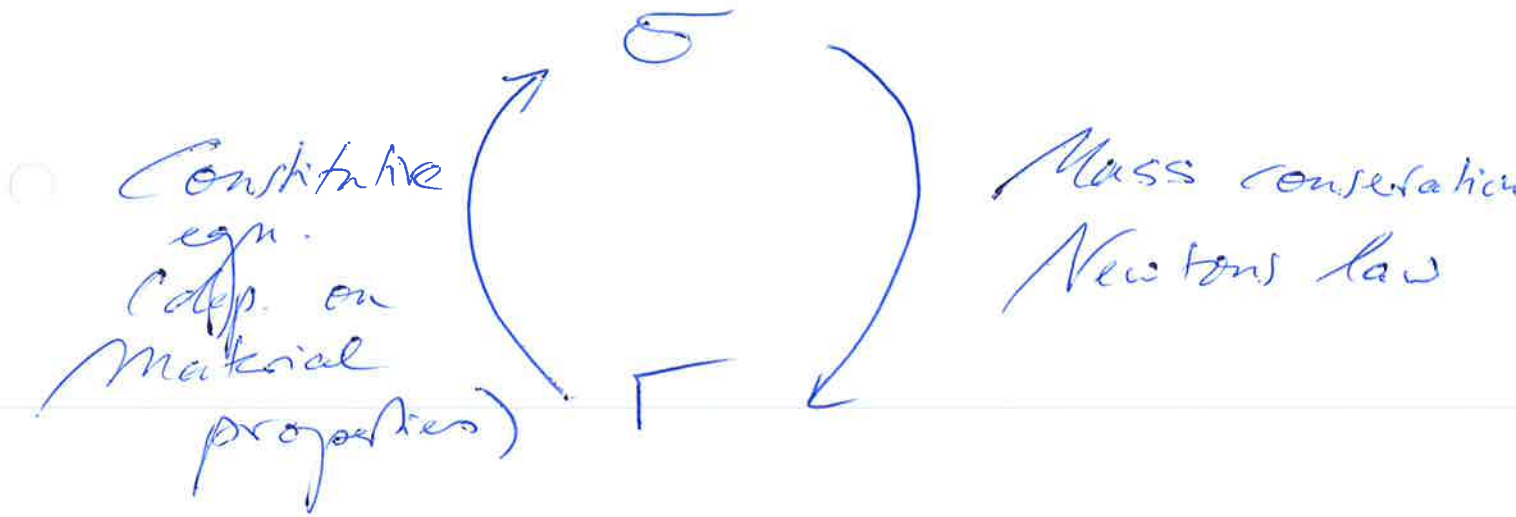


Couples to "deformations" of fluid elements, resulting in dissipation

How to couple

- stress \downarrow

- strain rate tensor ?




Mass Conservation

$\rho \underline{v} \equiv$ mass flux.

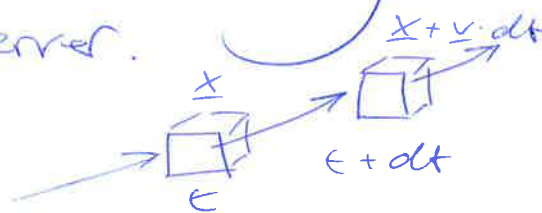
Partial time derivative. $\frac{\partial}{\partial t}$

... Measured by observer fixed in space.


$$\frac{\partial \rho}{\partial t} = -\nabla \cdot (\rho \underline{v}) = \underbrace{-\underline{v} \cdot \nabla \rho}_{\text{convection}} - \underbrace{\rho \nabla \cdot \underline{v}}_{\substack{\text{velocity} \\ \text{divergence} \\ \text{flux}}}.$$

Substantial time derivative $\frac{D}{Dt}$

... Measured by co-flowing observer.



$$\frac{D}{Dt} = \frac{\partial}{\partial t} + \underline{v} \cdot \nabla.$$

$$\frac{D\rho}{Dt} = \frac{\partial \rho}{\partial t} + \underline{v} \cdot \nabla \rho = -\rho \nabla \cdot \underline{v}$$

... lowest order of velocity field.

Momentum Conservation (Newton's law).

$$\rho \frac{Dv}{Dt} = \nabla \cdot \sigma + \underline{F}$$

mass-per-unit-volume
times
acceleration

↓
contact forces

body forces
(force volume density)

e.g. $\underline{F} = \rho \cdot \underline{g}$



$$\oint \sigma \cdot dS = \int \nabla \cdot \sigma \, dV$$

sum of
contact
forces



volume integral

Mass conservation + Momentum conservation

$$\begin{aligned}
 \frac{\partial(\rho \underline{v})}{\partial t} &= \frac{D(\rho \underline{v})}{Dt} - \underline{v} \cdot (\nabla \rho \underline{v}) \\
 &= \frac{D\rho}{Dt} \underline{v} + \rho \frac{D\underline{v}}{Dt} - \underline{v} \cdot (\nabla \rho \underline{v}) \\
 &\quad \downarrow \qquad \qquad \downarrow \\
 &= -\rho(\nabla \cdot \underline{v}) \underline{v} + \nabla \cdot \underline{\sigma} - \underline{v} \cdot (\nabla \rho \underline{v}) \\
 &= -\nabla(\rho \underline{v} \otimes \underline{v}) + \nabla \cdot \underline{\sigma} \\
 &= -\nabla \pi, \quad \pi = \rho \underline{v} \otimes \underline{v} - \underline{\sigma}
 \end{aligned}$$

$\frac{\partial(\rho \underline{v})}{\partial t} = -\nabla \pi$	Euler eqn.
---	---------------

Viscous stresses coupled to "deformations" of fluid elements result in the production of entropy

$S \equiv$ entropy per unit mass

$$\rho T \frac{Ds}{Dt} = \underbrace{\underline{\Gamma} : \underline{\sigma}'}_{\text{internal dissipation}} + \underbrace{k \nabla^2 T}_{\text{thermal conduction}}$$

(LL §49)

$\underline{\underline{\sigma}} \cdot \underline{n} \equiv$ contact forces

$$\oint \underline{v} \cdot \underline{\underline{\sigma}} \cdot \underline{n} = \int \underline{\nabla} \cdot (\underline{v} \cdot \underline{\underline{\sigma}}) \equiv \text{Work done by Contact forces (per unit volume \& unit time)}$$

$$\underline{\nabla} \cdot (\underline{v} \cdot \underline{\underline{\sigma}}) = \underbrace{-(\underline{\nabla} \cdot \underline{v}) \cdot p}_{\text{volume work}} + \underbrace{(\underline{\nabla} \underline{v}) : \underline{\sigma}'}_{\underline{\Gamma} : \underline{\sigma}' \text{ internal dissipation}} + \underbrace{\underline{v} \cdot (\underline{\nabla} \cdot \underline{\underline{\sigma}})}_{\text{work done in moving volume element as a whole}}$$

Onsager pair of "conj. variables"

$$\underline{\underline{\Gamma}} \text{ flux} \leftrightarrow \underline{\underline{\sigma}'} \text{ force}$$

Exploiting tensor symmetries

$$\sigma' = \frac{1}{3} \text{tr} \sigma' \mathbb{I} + \underbrace{\left(\sigma' - \frac{1}{3} \text{tr} \sigma' \mathbb{I} \right)}_{\Delta'}$$

$$\Gamma = \frac{1}{3} \underbrace{\text{tr} \Gamma \mathbb{I}}_{\underline{\nabla} \cdot \underline{v}} + \underbrace{\left(\Gamma - \frac{1}{3} \text{tr} \Gamma \mathbb{I} \right)}_{\Delta} \triangleq \text{shear rate tensor}$$

$$\sigma' : \Gamma = \frac{1}{3} \text{tr} \sigma' \mathbb{I} : \frac{1}{3} \text{tr} \Gamma \mathbb{I}$$

$$\frac{1}{3} \text{tr} \sigma' (\underline{\nabla} \cdot \underline{v})$$

energy dissipation due to volume change

$$+ \underbrace{\sigma' : \Delta}$$

energy dissipation due to shear deformations.

Constitutive equation

$$\sigma' = \sigma'(\Gamma)$$

- ideal fluid: $\sigma' = 0$.
- Newtonian fluid.

$$\sigma' = \text{lin. fun. of } \Gamma$$

$$\sigma'_{ij} = C_{ijke} \Gamma_{ke}$$

$$= k(\nabla \cdot v) \mathbb{I} + 2\gamma \Delta$$

↑
volume
viscosity

↑
shear
viscosity

Incompressible fluids $k \rightarrow \infty$:
 $\nabla \cdot v = 0$.

- Non-Newtonian fluids.
 - Shear softening Ketchup
 - Shear stiffening polymers
 - Memory

- Water $\gamma = 1.0 \frac{\text{pN} \cdot \text{ms}}{\mu\text{m}^2} @ 24^\circ\text{C}$

0.7 $\frac{\text{pN} \cdot \text{ms}}{\mu\text{m}^2} @ 36^\circ\text{C}$.

Navier-Stokes equation for incompressible Newtonian fluid.

• Euler eqn.

$$\frac{\partial(\rho \underline{v})}{\partial t} = -\nabla \cdot \underline{\underline{\Pi}}$$

$$\underline{\underline{\Pi}} = -\underline{\underline{\sigma}} + \rho \underline{v} \otimes \underline{v}$$

$$\underline{\underline{\sigma}} = -p \underline{\underline{I}} + \underline{\underline{\sigma}}$$

• Incompressible $\nabla \cdot \underline{v} = 0$
 $p(\underline{x}) = \text{const.}$

• Newtonian + incomp.

$$\underline{\underline{\sigma}} = 2\gamma \underline{\underline{\Delta}} = 2\gamma \underline{\underline{\Gamma}}$$

$$\rho \frac{\partial \underline{v}}{\partial t} = -\rho \underbrace{\nabla \cdot (\underline{v} \otimes \underline{v})}_{\substack{(\nabla \cdot \underline{v})\underline{v} + \underline{v} \cdot \nabla \underline{v} \\ = 0}} + \nabla p + 2\gamma \underbrace{\nabla \cdot \underline{\underline{\Gamma}}}_{\substack{\nabla \cdot \frac{1}{2}[\nabla \underline{v} + (\nabla \underline{v})^T] \\ = \frac{1}{2}[\nabla^2 \underline{v} + \nabla(\nabla \cdot \underline{v})] \\ = 0}}$$

$$\| \rho \frac{D \underline{v}}{D t} = \rho \left(\frac{\partial \underline{v}}{\partial t} + \underline{v} \cdot \nabla \underline{v} \right) = -\nabla p + \gamma \nabla^2 \underline{v}. \|$$

Hydrodynamic dissipation
for incompressible fluids.

Work done on fluid volume \rightarrow Compression
 \rightarrow Heat

$$\underline{v} \cdot \underline{\sigma} \cdot d\underline{s}$$


\equiv work done by contact force on surface element

$$* \oint \underline{v} \cdot \underline{\sigma} \cdot d\underline{s} = \int \nabla \cdot (\underline{v} \cdot \underline{\sigma}) d^3 \underline{r}$$

$$* \sigma = -p \mathbf{I} + 2\gamma \underline{\underline{\Gamma}}$$

$$* \nabla \cdot \sigma = -\nabla p \mathbf{I} + \nabla \cdot \gamma [\nabla \underline{v} + (\nabla \underline{v})^T]$$

$$= \underbrace{-\nabla p \mathbf{I} + \gamma \nabla^2 \underline{v}}_{=0} + \underbrace{\nabla \cdot (\nabla \cdot \underline{v})}_{=0}$$

$$\nabla \cdot (\underline{v} \cdot \underline{\sigma}) = (\nabla \underline{v}) : \underline{\sigma} + \underbrace{\underline{v} \cdot (\nabla \cdot \underline{\sigma})}_{=0}$$

$$= \nabla \underline{v} : (-p \mathbf{I} + 2\gamma \underline{\underline{\Gamma}})$$

$$= -p \nabla \cdot \underline{v} + 2\gamma \nabla \underline{v} : \underline{\underline{\Gamma}}$$

$$= 2\gamma \underline{\underline{\Gamma}} : \underline{\underline{\Gamma}}$$

Note: For compressible fluids, extra terms

Reynolds number

$$\rho \frac{Dv}{Dt} = -\nabla p + \mu \nabla^2 v + \rho F$$

L ... length-scale

v_0 ... velocity scale

$$\sim \rho \cdot v_0^2 / L$$

inertial forces

\sim

$$\mu v_0 / L^2$$

viscous forces

$$Re = \frac{\text{inertial forces}}{\text{viscous forces}} = \frac{\rho v_0^2 L}{\mu v_0 / L^2}$$

$$= \frac{\rho v_0 L}{\mu}$$

examples:

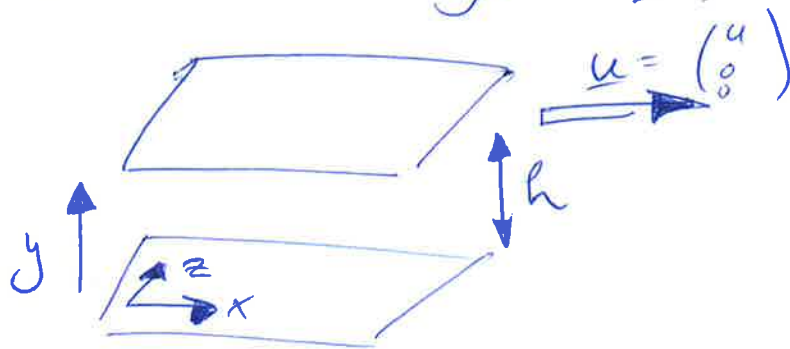
Sperm in Water

$$\rho = 1 \text{ g/cm}^3, \quad \mu = 10^{-3} \text{ Pa}\cdot\text{s} = 1 \frac{\text{pN}}{\mu\text{m}^2} \cdot \text{ms}$$

$$v_0 = 100 \mu\text{m/s}, \quad L = 100 \mu\text{m}$$

$$\rightarrow Re = \underline{\underline{10^{-2}}}$$

Scherströmung zwischen zwei Platten (LL § 17)



$$Re = 0: \quad 0 = -\nabla p + \gamma \sigma v. \quad (*)$$

Symmetrie: $p = p(y), \quad v = \begin{pmatrix} v_x(y) \\ 0 \\ 0 \end{pmatrix}$

$$0 = \begin{pmatrix} 0 \\ \partial_y p \\ 0 \end{pmatrix} + \gamma \begin{pmatrix} \partial_y^2 v_x \\ 0 \\ 0 \end{pmatrix} \quad (*')$$

$$\partial_y p = 0 \Rightarrow p = \text{const.}$$

$$v_x = ay + b. = \frac{y}{h} u.$$

$$\nabla v = \begin{pmatrix} 0 & u/h & 0 \\ 0 & 0 & 0 \\ 0 & 0 & 0 \end{pmatrix}$$

$$\sigma' = \frac{\gamma}{2} [\nabla v + (\nabla v)^T] = \begin{pmatrix} 0 & u/2h & 0 \\ u/2h & 0 & 0 \\ 0 & 0 & 0 \end{pmatrix}$$

$$\sigma = -p \mathbb{I} + \sigma'$$

$$\sigma_{yy} = p$$

$$\sigma_{xy} = \frac{\gamma u}{2h}$$

Reminder:

Incompressible
Newtonian fluid.

$$\nabla \cdot \mathbf{v} = 0.$$

$$\nabla \sigma' = \mu \nabla \Gamma = 0.$$

$$\sigma' = \sigma' - \frac{1}{3} \nabla \sigma' \cdot \mathbf{I} \mathbf{I} = 2\mu \Delta = 2\mu \left(\Gamma - \frac{1}{3} \nabla \Gamma \right)$$

$$Re = \frac{\rho v_0 L}{\mu}.$$

§ 17

Strömung durch ein Rohr.



$$V = \begin{pmatrix} V_x(r) \\ \vdots \\ \vdots \end{pmatrix}$$

$$\partial_y p = \partial_z p = 0 \Rightarrow p = p(x)$$

$$\frac{\partial^2 V_x}{\partial y^2} + \frac{\partial^2 V_x}{\partial z^2} = \frac{1}{3} \frac{dp}{dx}$$

dep. only on y, z dep. only on x :

$$\Rightarrow \frac{dp}{dx} = \text{const.} = - \frac{\Delta p}{L}$$

Laplace operator in polar coords:

$$- \frac{\Delta p}{3L} = \Delta V = \frac{1}{r} \partial_r (r \partial_r V_x)$$

$$- \frac{\Delta p}{23L} r^2 + a = r \partial_r V_x$$

simple
integration

$$- \frac{\Delta p}{43L} r^2 + \underbrace{a \ln r + b}_{\text{singularity at } r=0} = V_x$$

singularity at $r=0$.

$$\Rightarrow V_x = \frac{\Delta p}{43L} (R^2 - r^2)$$

flux

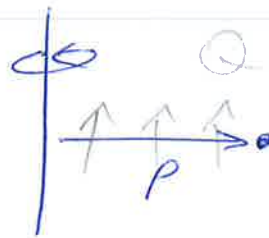
$$Q = 2\pi r \int_0^R r V_x dr$$

$$= \frac{\pi r \Delta p}{83L} R^4$$

Poiseuillesches Gesetz.

Tricks to solve flow problems at low Re

- potential flow = irrotational flow with $\nabla \times \underline{v} = 0$
 $\Rightarrow \underline{v} = \nabla \Phi$
 \Rightarrow solve equation for Φ (harmonic functions)
- axisymmetric flow



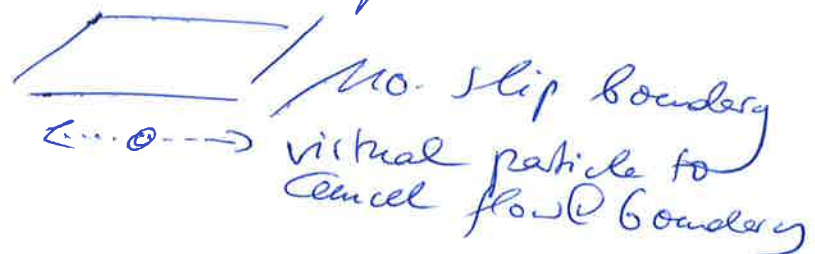
$$\psi = \frac{Q}{2\pi r}$$

\Rightarrow equation for ψ

- 2D flow problems: formulate in terms of single complex coordinate.

- conformal mappings $z \mapsto zu$

- fundamental singularities
- methods of images



Stokes equation

$$\mathbf{0} = -\nabla p + \mu \nabla^2 \underline{v} + \underline{F}$$

- linear PDE.
- fundamental solution = Oseen tensor

$$G_{ij} = \frac{1}{8\pi\eta} \cdot \frac{1}{r} (\delta_{ij} + \hat{r}_i \otimes \hat{r}_j)$$

\equiv flow due to a point force

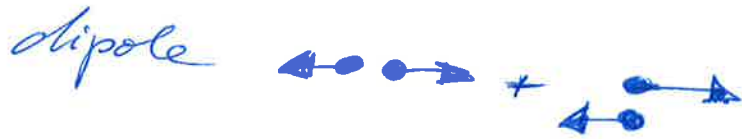
\equiv Stokes let.

$$\underline{v} = \underline{G} \cdot \underline{F}$$



$$p = \frac{1}{4\pi} \frac{\underline{r} \cdot \underline{F}}{|\underline{r}|^3}$$

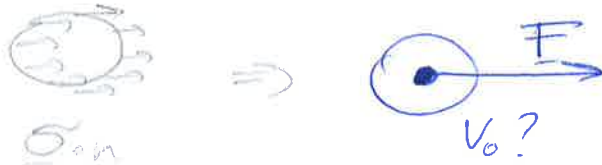
- spatial derivatives of Oseen tensor also solutions of Stokes equation



quadrupole ...

Drag on a sphere

Surface forces
 σ_{in}



- Construct solution from superposition of fundamental solutions
- flow axisymmetric & mirror symmetric w.r.t y^2 -plane
- Stokes let $= 6\pi\eta R$

Stokes doublet (dipole)



- Stokes quadrupole

flow field around a ~~moving~~ translating sphere

$$v_i = \left(1 + \frac{a^2}{6} \nabla^2\right) \delta_{ij} \underline{F}_j$$

$$p = \frac{1}{4\pi} \frac{\underline{r} \cdot \underline{F}}{r^3} \equiv \text{decays quadratically}$$

Stress tensor

$$\underline{\sigma} = -p \underline{I} + 2\gamma \underline{\tau}$$

traction force

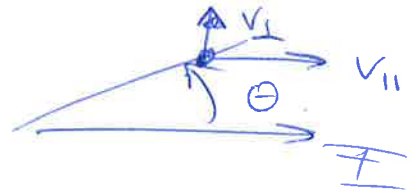
$$\underline{\sigma} \cdot \underline{n} = -\frac{1}{4\pi a^2} \underline{F} \quad \leftarrow \text{Diagram of a sphere with arrows pointing outwards}$$

Surface force density exerted by fluid
↳ individual contributions

- p and $2\gamma \underline{\tau}$ more complicated

Oseen tensor in spherical coords.

$$v_i = G_{ij} \cdot F_j$$



Stokes let = axisymmetric flow

$$V_{||}^{(1)} = \frac{3 + \cos 2\theta}{16\pi\eta r} f_0 \quad \xrightarrow{2x} \quad \xrightarrow{2x}$$

$$V_{\perp}^{(1)} = \frac{3 \sin 2\theta}{16\pi\eta r} f_0$$

Laplacian of Oseen tensor

$$V_{||}^{(3)} = -\frac{1 + 3 \cos 2\theta}{8\pi\eta a^3} \alpha f_0$$

$$V_{\perp}^{(3)} = -\frac{3 \sin 2\theta}{8\pi\eta a^3} \alpha f_0$$

$$\alpha = \frac{a^2}{6}$$

$$\text{at } r=a: \quad v_{||} = V_{||}^{(1)} - \alpha V_{||}^{(3)} = \frac{1}{6\pi\eta a} f_0$$

$$v_{\perp} = V_{\perp}^{(1)} - \alpha V_{\perp}^{(3)} = 0$$

$$\underline{\underline{F = 6\pi\eta a v_0}}$$

Multipole gymnastics

Reminds: electrostatic: charge distribution
dominates ← - net charge \oplus
far-field - dipole $\oplus \ominus$
- quadrupole $\oplus \ominus \oplus \ominus$
- ...

We are dealing with force fields.

$$f_i(\underline{r}) = \sigma_{ij} \cdot n_j$$



Monopole = net force

surface density of forces

$$F_{tot,i} = \int_S d^2\underline{r} f_i(\underline{r})$$

Cartesian multipole moments

$$f_{j,\alpha} = \int_S d^2\underline{r} (\underline{r} - \underline{r}_0)^\alpha f_j(\underline{r})$$

Multipole expansion

$$f_j(\underline{r}) = \sum_{\alpha} \frac{(-1)^{|\alpha|}}{\alpha!} f_{j,\alpha} \nabla^\alpha \delta(\underline{r} - \underline{r}_0)$$

check:

$$\begin{aligned} f_{j,\alpha} &= \int_S d^2\underline{r} (\underline{r} - \underline{r}_0)^\alpha \sum_k \frac{(-1)^k}{k!} f_{j,k} \nabla^k \delta(\underline{r} - \underline{r}_0) \\ &= f_{j,\alpha} \end{aligned}$$

Recursive flow field:

$$v_i(\underline{r}) = \int d\underline{r}' G_{ij}(\underline{r}-\underline{r}') f_j(\underline{r}') \\ = \sum_{\alpha} \frac{(-1)^{\alpha}}{\alpha!} G_{ij,\alpha}(\underline{r}-\underline{r}_0) f_{j,\alpha}.$$

Special case: sphere of radius a



Relation between Multipoles,

e.g.

$$f_{j,xx} + f_{j,yy} + f_{j,zz} = a^2 f_j$$

one (out of several)

trace of rank-3-tensor.

N.B.

These trace-relations are the only relations between Multipoles (rank $k \leftrightarrow$ rank $k+2$).

The "trace-less" tensors are independent and can be mapped on expansion into spherical harmonics.

Deep relation to representation theory of $SO(3)$

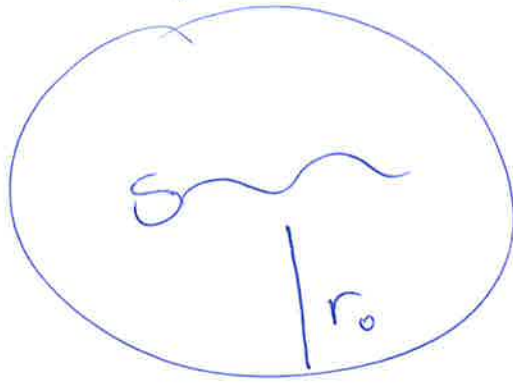
Application:

Flow field of a sphere

$$v_j = G_{ij} (r - r_0) F_j + \frac{a^2}{6} \nabla^2 G_{ij} (r - r_0) F_j + \dots$$

In fact: "... is zero, $\nabla^4 G_{ij} = 0$.

Thought experiment



- remove swimmer +
fluid sphere $|r| \leq r_0$

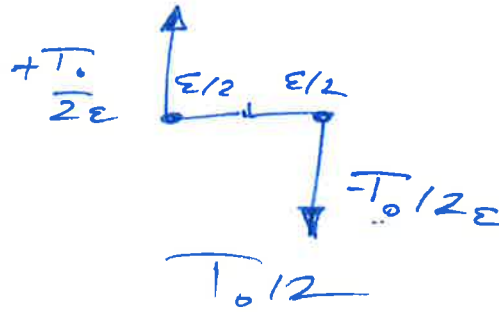
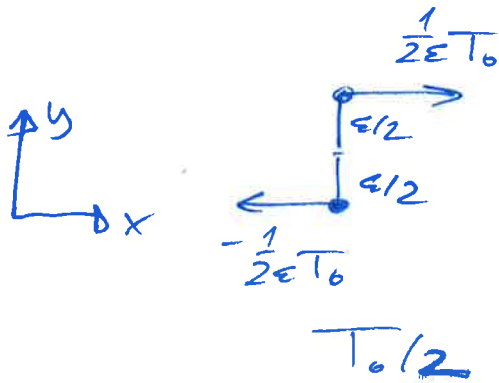
- add surface force density
 $\sigma(\underline{r}) \cdot \delta(|r| - r_0)$

→ same flow field outside

Rotation of a sphere



$\underline{I} = T_0 \underline{e}_z \equiv$ external angular momentum



force dipole representation

$$G_{ix,y} T_{0/2}$$

$$- G_{iy,x} T_{0/2}$$

flow field.

$$\text{Stokes } G_{ix,y} = \begin{pmatrix} -y/r^3 \\ 0 \\ 0 \end{pmatrix} - 3 \begin{pmatrix} x^2 \\ xy \\ xz \end{pmatrix} \frac{y}{r^5} + \begin{pmatrix} 0 \\ x/r^3 \\ 0 \end{pmatrix}$$

$$V_i = G_{ix,y} T_{0/2} - G_{iy,x} T_{0/2}$$

$$= \frac{r_i}{r^3} \epsilon_{ijz} \frac{T_0}{4\pi\eta}$$

$$\omega = \frac{T_0}{4\pi\eta a^2}$$

$$8\pi\eta a^3 \cdot \omega = T_0$$

~~Flow in a pipe~~

Einstein relation

$$D_{\text{trans}} = \frac{k_B T}{6\pi\eta a} \quad \left[\frac{\text{m}^2}{\text{s}} \right]$$

$$D_{\text{rot}} = \frac{k_B T}{8\pi\eta a^3} \quad \left[\frac{1}{\text{s}} \right]$$

Example:

$$a = 1 \mu\text{m}$$

$$\eta = 1 \frac{\text{pN} \cdot \text{ms}}{\mu\text{m}^2}$$

$$k_B T = 4 \cdot 10^{-21} \text{ J} \\ = 4 \text{ pN} \cdot \mu\text{m}$$

$$D_{\text{trans}} = 0.2 \frac{\mu\text{m}^2}{\text{s}}$$

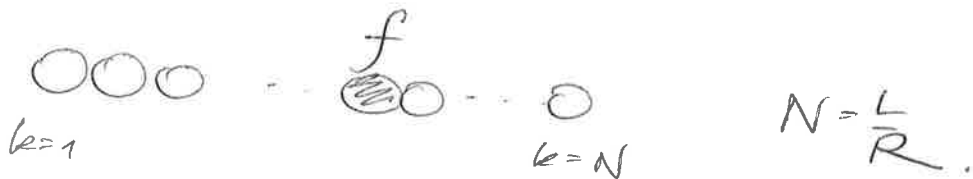
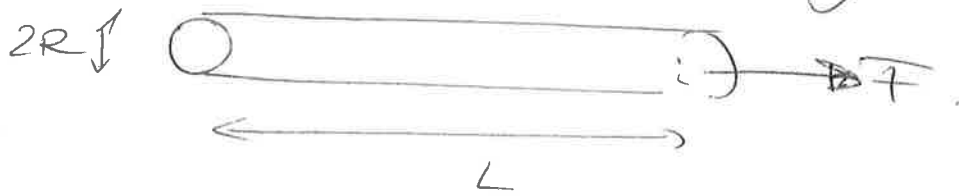
$$D_{\text{rot}} = 0.15 \frac{1}{\text{s}} \sim \frac{1}{6 \text{ sec}}$$

Swimming

E. coli:

- transl. diffusion negligible
 - rot. diffusion randomizes swimming direction within ca. 10 sec.
- adopted navigation

Drag on a translating cylinder



$$f \approx \frac{F}{N}$$

$$f = 6\pi\eta R [v_{II} - v_{fluid}]$$

$$v_{fluid} = \sum_{\substack{k=1 \\ k \neq N/2}}^N \frac{f}{6\pi\eta R} \frac{2}{|x_k - x_{N/2}|}$$

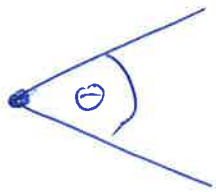
$$2 \int_0^{L/2-R} \frac{1}{|x - L/2|} dx$$

$$2 [-\ln(L/2 - x)]_0^{L/2-R} = 2 [-\ln R + \ln L/2] = 2 \ln \frac{L}{2R}$$

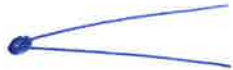
$\gg v_0$ for $L \gg R$.

$$F_{II} = \sum_{II} v_{II}, \quad \sum_{II} = \frac{4\pi\eta L}{2 \ln \frac{L}{2R}}, \quad F_{\perp} = \sum_{\perp} v_{\perp}, \quad \sum_{\perp} = 2\sum_{II}$$

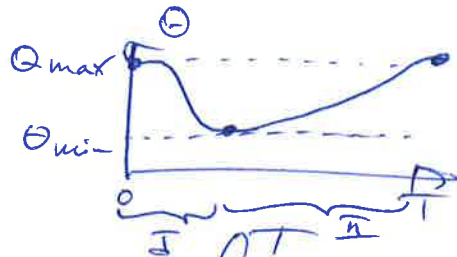
Parcell's Scallop.



single hinge



$$V_x = g(\theta) \dot{\theta}$$



$$\bar{V} = \int_0^T dt V_x(t) = \int_0^T dt g(\theta) \dot{\theta}$$

$$= \underbrace{\int_{\theta_{min}}^{\theta_{max}} d\theta g(\theta)}_{II} - \underbrace{\int_{\theta_{min}}^{\theta_{max}} d\theta g(\theta)}_I$$

$$= 0$$

You cannot swim with
1 (linear) degree of freedom.

N.B.

With 2 DOF, net propulsion becomes possible!

$$DOF \neq 1 \Rightarrow$$

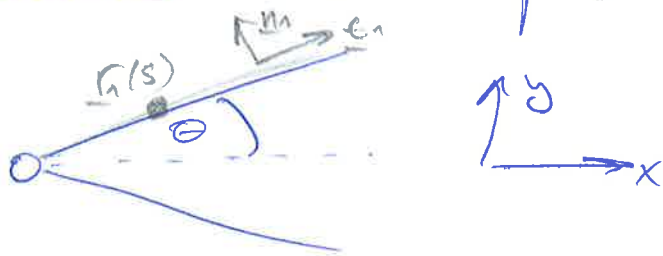
$$DOF \neq 2 \Rightarrow$$

\Rightarrow Non-linear hydro. int. between DOFs

$$\Rightarrow \nabla \neq 2$$

Oblique swims: two-steps-forward, one-step-back

Purcell's Scallop



$$\underline{r}_1(s) = s \underline{e}_1, \quad \underline{e}_1 = \begin{pmatrix} \cos \theta \\ \sin \theta \end{pmatrix}$$

$$\underline{n}_1 = \begin{pmatrix} -\sin \theta \\ \cos \theta \end{pmatrix}$$

- rigid body motion in x-direction

$$\underline{v} = v_0 \begin{pmatrix} 1 \\ 0 \end{pmatrix}$$

$$f_1(s) = \xi_{\parallel} (\underline{v} \cdot \underline{e}_1) \underline{e}_1 + \xi_{\perp} (\underline{v} \cdot \underline{n}_1) \underline{n}_1$$

$$= \xi_{\parallel} v_0 \cos \theta \begin{pmatrix} \cos \theta \\ \sin \theta \end{pmatrix} + \xi_{\perp} \begin{pmatrix} -\sin \theta \\ \cos \theta \end{pmatrix} (-\sin \theta) v_0$$

$$\underline{F}_{\text{tot}} = \int_0^L ds f_1(s) + f_2(s)$$

$$= \left(\xi_{\parallel} v_0 L \cdot 2 \cos^2 \theta + \xi_{\perp} v_0 L \cdot 2 \sin^2 \theta \right)$$

- forces exerted for shape change,
motion of pivot point constrained

$$\underline{v}_1 = \dot{\theta} s \underline{n}_1$$

$$f_1(s) = \xi_{\perp} s \cdot \underline{n}_1 \cdot \dot{\theta}$$

$$F_{\text{tot}} = 2 \xi_{\perp} L^2 / 2 \dot{\theta} \sin \theta$$

- force balance

$$: 2 \xi_{\parallel} v_0 L (\xi_{\parallel} \cos^2 \theta + \xi_{\perp} \sin^2 \theta) + - \dot{\theta} L^2 \xi_{\perp} \sin \theta$$

$$\Rightarrow v_0 = + \frac{L}{2} \frac{\xi_{\perp} \sin \theta}{\xi_{\parallel} \cos^2 \theta + \xi_{\perp} \sin^2 \theta} \dot{\theta} = g(\theta) \dot{\theta}$$

Bacterial Swimming

CCW-helix.

ω



CCW-rotation



$$r(s) = \left(r_0 \cos\left(\frac{s}{\sqrt{r_0^2 + l_0^2}} + \omega t\right), r_0 \sin\left(\frac{s}{\sqrt{r_0^2 + l_0^2}} + \omega t\right), l_0 s + v_0 t \right)$$

$$r_0 = l \cos \theta, \quad l_0 = l \sin \theta.$$

$\theta =$ helix angle

- pure rotation for $v_0 = 0$

$$\overline{F_{\omega, z}} = \int_0^L ds f(s) \cdot \underline{e}_z = \text{thrust force for constrained cell body}$$

at $s=0$:

$$\underline{t} = (0, \cos \theta, \sin \theta)$$

$$\underline{v} = (0, -l\omega, 0)$$

$$v_{||} = (0, *, -r_0 \omega \cos \theta \sin \theta)$$

$$v_{\perp} = (0, *, r_0 \omega \cos \theta \sin \theta)$$

$$f(s=0) = \gamma_{||} v_{||} + \gamma_{\perp} v_{\perp} = (0, *, \frac{\gamma_{||} - \gamma_{\perp}}{2} \frac{r_0 \omega}{\sin 2\theta})$$

$$\overline{F_{\omega, z}} = \frac{\gamma_{||} - \gamma_{\perp}}{2} r_0 \omega \cdot L \cdot \sin 2\theta$$

- pure translation with $\omega=0$.

$$\underline{V} = (0, 0, v_0)$$

$$\underline{V}_{\parallel} = (0, *, v_0 \sin^2 \theta)$$

$$\underline{V}_{\perp} = (0, *, v_0 \cos^2 \theta)$$

$$\begin{aligned} f(s=0) &= \underline{I}_{\parallel} \underline{V}_{\parallel} + \underline{I}_{\perp} \underline{V}_{\perp} \\ &= v_0 (0, *, \underline{I}_{\parallel} \sin^2 \theta + \underline{I}_{\perp} \cos^2 \theta). \end{aligned}$$

$$\begin{aligned} \tau_{\text{trans}, z} &= L \cdot v_0 (\underline{I}_{\parallel} \sin^2 \theta + \underline{I}_{\perp} \cos^2 \theta) \\ &\quad + 6\pi \eta a v_0 \end{aligned}$$

- force balance

$$v_0 = \frac{(\underline{I}_{\perp} - \underline{I}_{\parallel}) \Gamma \sin 2\theta \cdot v_0}{\underline{I}_{\parallel} \sin^2 \theta + \underline{I}_{\perp} \cos^2 \theta + 6\pi \eta a L}$$

$$\omega \neq \omega_0$$

Counts-rotation of cell

• torque balance

$$0 = \overline{T}_{\text{flag}} + \overline{T}_{\text{cell}}$$

$$\overline{T}_{\text{cell}} = \pi \gamma a^3 (\omega - \omega_0) \underline{e}_z$$

$$\overline{T}_{\text{flag}} = \int_0^L \underline{f}(s) \times \underline{r}(s) ds$$

$$0 = \pi \gamma a^3 (\omega - \omega_0) + \omega \cdot L r_0^2 \cdot g(\underline{s}_{||}, \underline{s}_{\perp}, \theta, \frac{\pi \gamma a^2}{L})$$

$$\omega = \omega_0 \frac{1}{1 + \frac{L r_0^2}{\pi \gamma a^3} g(\underline{s}_{||}, \underline{s}_{\perp}, \theta, \frac{\pi \gamma a^2}{L})}$$

- At large Re , viscosity negligible: Vogel ch. 4
Ideal fluid def'd as $\gamma=0$.
- In ideal fluids, Bernoulli's principle holds.

$$\rho \frac{Dv}{Dt} = -\nabla p.$$

mass \times acceleration pressure force

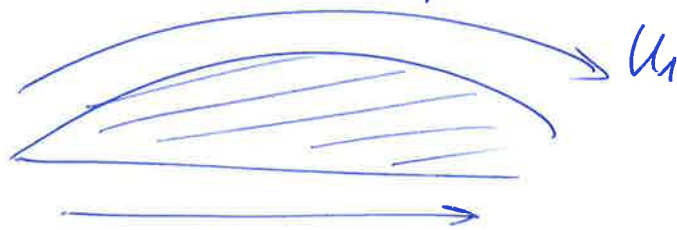
$$dt = dl/v$$

$$\rho \frac{dv}{dt} = \rho \frac{dv \cdot v}{dl} = -\frac{dp}{de}$$

$$\frac{1}{2} v^2 + p = \text{const}$$

→ generalization to vector case: Euler equation (LL)

- Why does an airplane fly?

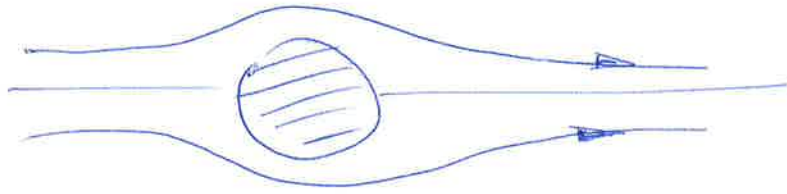


$$\frac{1}{2}(u_1^2 - u_2^2) + (p_1 - p_2) = 0.$$

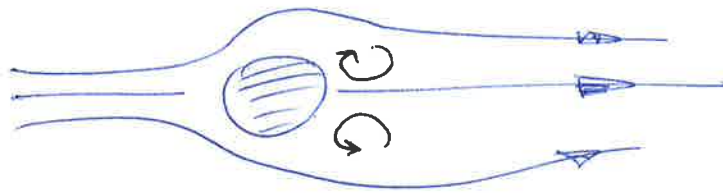
$$u_1 > u_2 \Rightarrow p_1 < p_2 \Rightarrow \text{lift}.$$

- close to boundary:
viscosity not negligible
→ boundary layer, turbulence

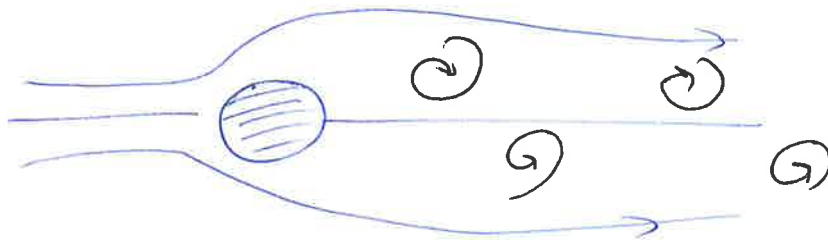
Creeping flow ($Re < 10$).



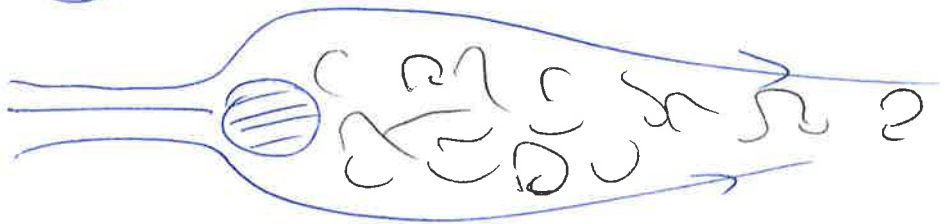
Attached vortices ($10 < Re < 40$).



Van Karman vortex trail ($40 < Re < 2 \cdot 10^5$).



Fully turbulent wake ($Re > 2 \cdot 10^5$).



Shore waves

Conservation of Circularity

$\gamma = 0$: ideal fluid.

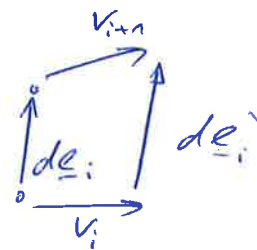


$$\frac{Dv}{Dt} = -\frac{1}{\rho} \nabla p.$$

$$\oint_c \underline{v} \cdot d\underline{e} = \underbrace{\nabla \times \underline{v}}_{\text{vorticity}} \cdot d\underline{A} = \text{circularity.}$$

$$\frac{d}{dt} \oint_{c(t)} \underline{v} \cdot d\underline{e} \quad \begin{array}{l} - \underline{v} \text{ changes} \\ - c \text{ changes.} \end{array}$$

$$= \frac{d}{dt} \oint_{c(t)} \underline{v} \cdot d\underline{e} + \oint \underline{v} \cdot \frac{d}{dt} d\underline{e}$$



$$= \frac{d}{dt} (\nabla \times \underline{v}) \cdot d\underline{A} + \oint \underline{v} \cdot \frac{d}{dt} d\underline{e} = \frac{d}{dt} (\nabla \times \underline{v}) \cdot d\underline{A} + \oint \frac{d}{dt} \underline{v} \cdot d\underline{e} = 0$$

integral of total differential
(change in \underline{v} and $d\underline{e}$ cancel).

$$= \nabla \times \left(\frac{d}{dt} \underline{v} \right) \cdot d\underline{A}$$

$$= \nabla \times \left(-\frac{1}{\rho} \nabla p \right) \cdot d\underline{A}$$

$$= 0$$

Thomson's law.

Navier-Stokes (Newtonian fluid, incompressible)

$$\rho \left[\frac{\partial \underline{v}}{\partial t} + \underline{v} \cdot (\underline{\nabla} \otimes \underline{v}) \right] = -\underline{\nabla} p + \eta \nabla^2 \underline{v}$$

vector identity

$$\underline{v} \cdot (\underline{\nabla} \otimes \underline{v}) = \frac{1}{2} \underline{\nabla} |\underline{v}|^2 - \underline{v} \times (\underline{\nabla} \times \underline{v})$$

Take $\underline{\nabla} \times$ on both sides.

$$\rho \left[\frac{\partial \underline{\omega}}{\partial t} - \underline{\nabla} \times (\underline{v} \times \underline{\omega}) \right] = 0 + \eta \nabla^2 \underline{\omega}$$

another vector identity

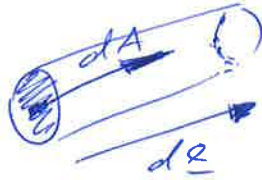
$$\underline{\nabla} \times (\underline{v} \times \underline{\omega}) = -\underline{v} \cdot (\underline{\nabla} \otimes \underline{\omega}) + \underline{\omega} \cdot (\underline{\nabla} \cdot \underline{v})$$

using $\underline{\nabla} \cdot \underline{v} = 0, \underline{\nabla} \cdot \underline{\omega} = 0.$

$$\frac{D \underline{\omega}}{Dt} = \underbrace{\underline{\omega} \cdot (\underline{\nabla} \otimes \underline{v})}_{\substack{\text{change of} \\ \text{vorticity} \\ \text{perpendicular} \\ \text{to streamline}}} + \frac{\eta}{\rho} \nabla^2 \underline{\omega}.$$

Revisit Thomson's law.

$$0 = \frac{D}{Dt} \underline{\omega} \cdot d\underline{A}$$



$$dV = d\underline{A} \cdot d\underline{L}$$

$$0 = \frac{D}{Dt} dV = \frac{D}{Dt} (d\underline{A} \cdot d\underline{L})$$

$$= \left(\frac{D}{Dt} d\underline{A} \right) \cdot d\underline{L} + \underbrace{\left(\frac{D}{Dt} d\underline{L} \right)}_{d\underline{L} \cdot (\nabla \otimes \underline{v})} \cdot d\underline{A}$$

Must hold for all $d\underline{L}$

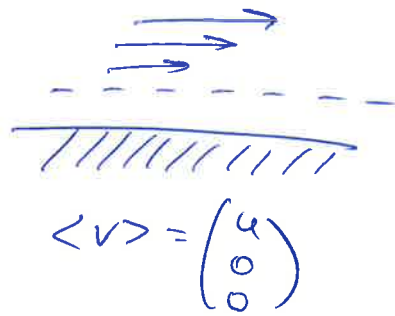
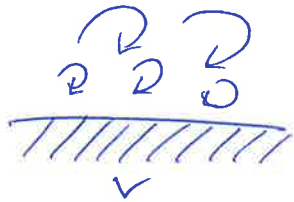
$$\frac{D}{Dt} d\underline{A} = -(\nabla \otimes \underline{v}) \cdot d\underline{A}$$

$$\begin{aligned} \frac{D}{Dt} \underline{\omega} \cdot d\underline{A} &= \underline{\omega} \cdot (\nabla \otimes \underline{v}) \cdot d\underline{A} + \frac{\gamma}{\rho} (\nabla^2 \underline{\omega}) \cdot d\underline{A} \\ &\quad - \underline{\omega} (\nabla \otimes \underline{v}) \cdot d\underline{A} \end{aligned}$$

$$= \frac{\gamma}{\rho} (\nabla^2 \underline{\omega}) \cdot d\underline{A}$$

$$= 0 \text{ for } \gamma = 0.$$

The logarithmic velocity profile $u \propto \ln y$



$$\langle v \rangle = \begin{pmatrix} u \\ 0 \\ 0 \end{pmatrix}$$

• $\sigma_{xy} : \frac{N}{m^2} = \frac{kg \cdot m/s}{s \cdot m^2} = \text{momentum flux}$

$$v^* = \sqrt{\sigma_{xy} / \rho}$$

• $u = u(y)$

$$\frac{\partial u}{\partial y} = f(\sigma, \rho, y) = \frac{1}{\kappa} \frac{v^*}{y}, \quad \kappa = 0.4$$

$$u = \frac{v^*}{\kappa} \ln(y/c)$$

What is c ?

• Viscous boundary layer.

$$Re = \rho \frac{v^* y_0}{\mu}$$

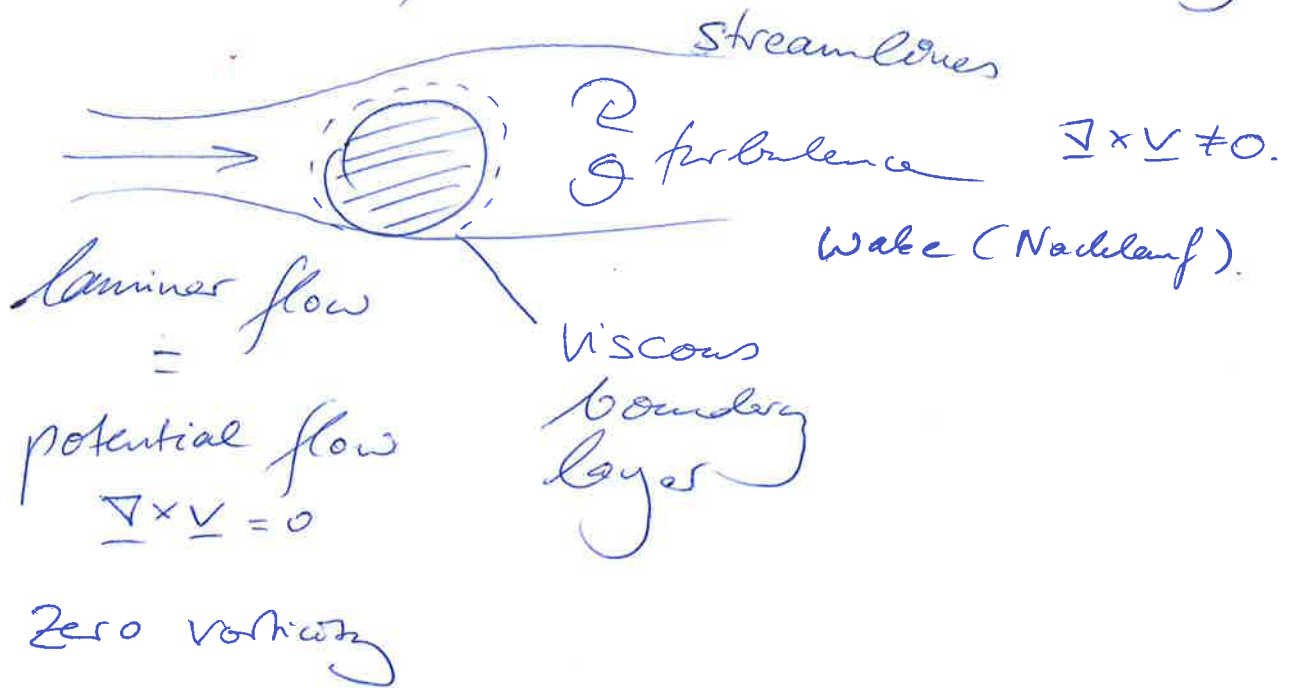
$$Re \sim 1 \Rightarrow y_0 \sim \frac{\mu}{\rho v^*}$$

$$y \ll y_0: u = \frac{\sigma}{\mu} y = \frac{\rho v_*^2}{\mu} y \Rightarrow u \sim v_* \ln(y/y_0)$$

• Matching near and far-field

$$u = \frac{v^*}{\kappa} \ln\left(\frac{y}{y_0}\right) = \text{log. velocity profile}$$

Turbulent flow around a body

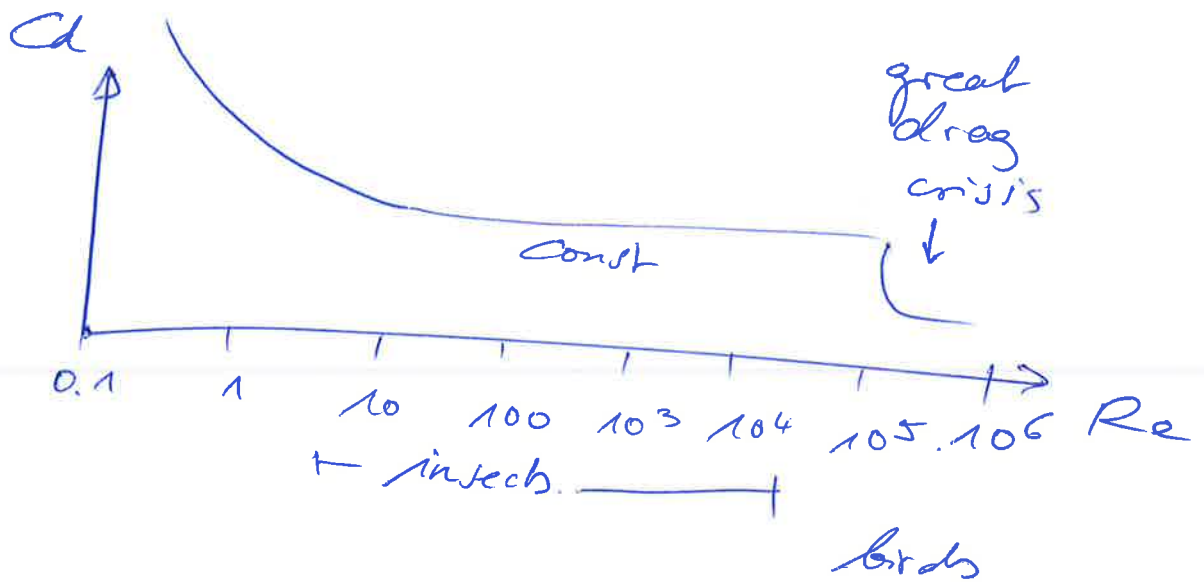


$$F = \text{const.} \rho u^2 L^2 \quad Re \gg 1.$$

$$= \text{const.} \gamma \cdot u \cdot L \quad Re \ll 1.$$

Drag coefficients and the Reynolds number.

$$F_{\text{drag}} = \left(\frac{1}{2} \rho A u^2 \right) \cdot C_d(Re).$$

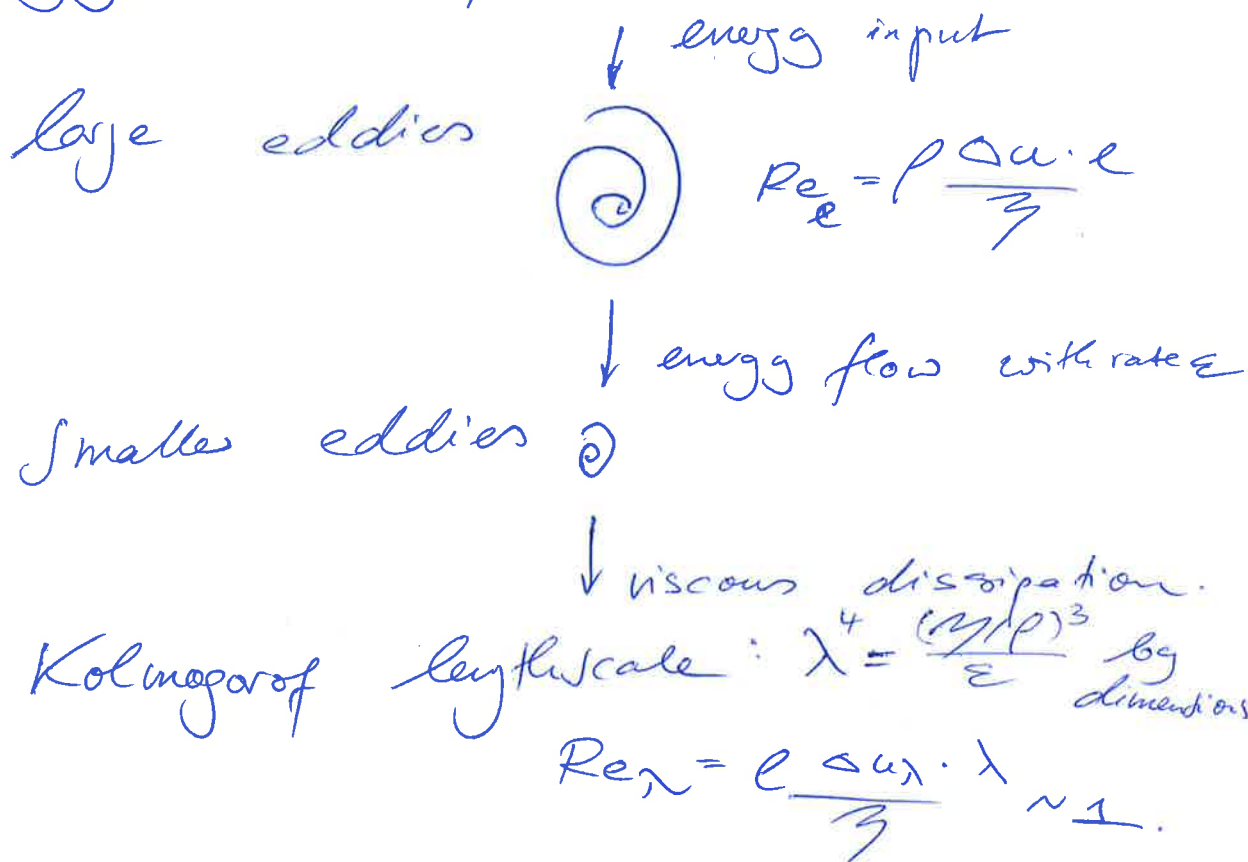


skin friction dominates.

pressure drag:
fluid accelerated to flow around body; drag not so high but dissipated

turbulence invades boundary layers. Separation line moves forward.

Energy dissipation.



rate of energy flow

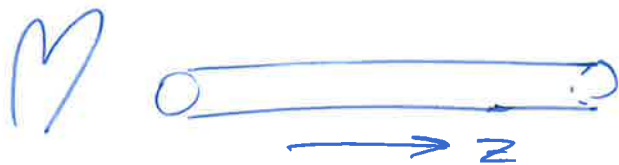
$$\epsilon \sim \frac{(\Delta u_e)^3}{l}$$

$[\frac{N}{kg \cdot s}]$ by dimensions.

ϵ constant across scales.

$$\Delta u_e \sim l^{1/3} \equiv \text{self-similarity.}$$

$$\rho \frac{\partial v}{\partial t} = -\nabla p + \eta \nabla^2 v \quad (*)$$



$$\frac{\partial p}{\partial z} = p_0 \exp i\omega_0 t$$

Ansatz $v = u(r) \exp i\omega_0 t e_z$.

(*) gives:

$$\rho i\omega_0 u = -p_0 + \eta \left(u_{rr} + \frac{1}{r} u_r \right)$$

Laplace op. polar coords



$$u(r) = \frac{i p_0}{\rho \omega_0} \left(1 - \frac{\mathcal{E}_0(i^{3/2} \alpha r/R)}{\mathcal{E}_0(i^{3/2} \alpha)} \right)$$

$$\alpha = \sqrt{\frac{\omega_0 \rho}{\eta}} R \equiv \text{Womersley number}$$

$$\text{flux} = 2\pi \int_0^R u(r) r dr$$

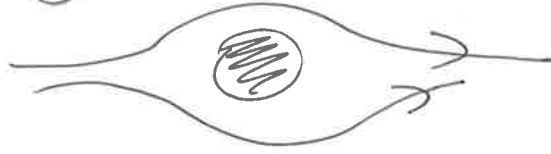
$= 15$ aorta
 5 arteries
 0.05 arterioles
 0.005 capillaries

$$\frac{-i \sqrt{\pi} p_0 R^4}{\eta} \frac{\exp i\omega_0 t}{\alpha^2} \frac{\mathcal{E}_2(i^{3/2} \alpha)}{\mathcal{E}_0(i^{3/2} \alpha)}$$

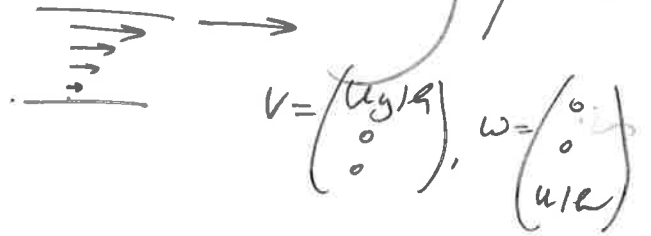
$$= \begin{cases} \frac{\sqrt{\pi} p_0 R^4}{8\eta} & |\alpha| \ll 1 \\ \frac{\sqrt{\pi} p_0 R^2}{\omega_0 \rho} & |\alpha| \gg 1 \end{cases}$$

$Re = 0$ viscous flow.

(creeping flow, Stokes flow)



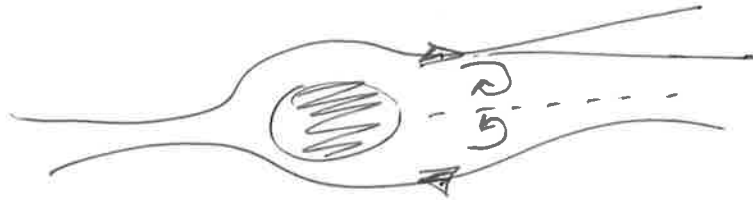
laminar. = streamlines locally parallel



2000 - 5000.

turbulent

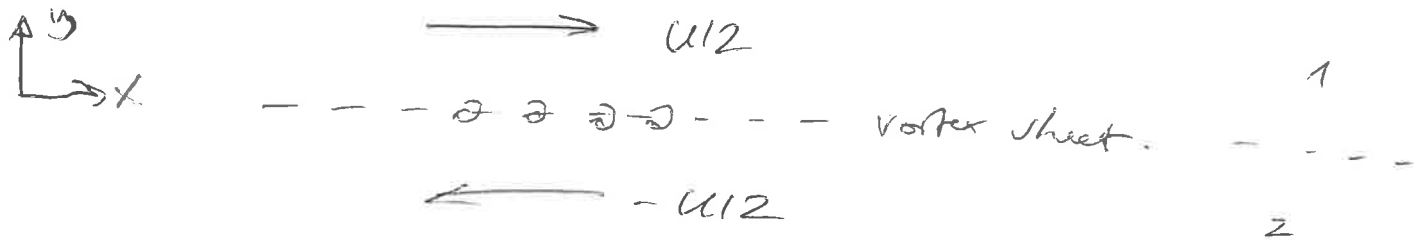
- chaotic (\Rightarrow mixing).
- unsteady vortices.
- $\omega \neq 0$.



$Re = \infty$: ideal fluid: inviscid flow.

- Steady / unsteady.

Instabilities of flows



- Ideal fluid ($\nu=0$): infinitesimal thin boundary layer
- Q: Will the boundary layers remain straight?
 $h = h(x, t) =$ height profile
- In the upper/lower half-space flow \rightarrow laminar and irrotational $\omega=0$.

potential flow $v = \nabla \psi$

$$\psi_1 = +\frac{u}{2}x + \phi_1$$

$$\psi_2 = -\frac{u}{2}x + \phi_2$$

- h, ϕ_1, ϕ_2 coupled:

$$v_y^{(1)} = \frac{\partial \phi_1}{\partial y} \Big|_{y=0} = \frac{Dh}{Dt} \Big|_{y=0} \approx \frac{\partial h}{\partial t} - \frac{1}{2}u \frac{\partial h}{\partial x} \quad (1)$$

$$v_y^{(2)} = \frac{\partial \phi_2}{\partial y} \Big|_{y=0} = \frac{Dh}{Dt} \Big|_{y=0} \approx \frac{\partial h}{\partial t} + \frac{1}{2}u \frac{\partial h}{\partial x} \quad (2)$$

- 2nd equation from pressure difference.
- generalize Bernoulli's principle

$$-\frac{Dv}{Dt} = -\frac{1}{\rho} \nabla p \quad \equiv \text{Navier-Stokes for incompressible, ideal fluid}$$

$$= \frac{\partial v}{\partial t} + v \cdot (\nabla \otimes v)$$

- Vector identity

$$\frac{1}{2} \nabla (v \cdot v) = \underline{v} \cdot \nabla \underline{v} + \underline{v} \times \underline{\omega}$$

$$- v = \nabla \psi, \quad \omega = 0.$$

$$- \nabla \left(\frac{\partial \psi}{\partial t} + \frac{1}{2} |v|^2 + \frac{p}{\rho} \right) = 0.$$

[Batchelor (6.25)]

$$\rightarrow \frac{\partial \psi}{\partial t} + \frac{1}{2} |v|^2 + \frac{p}{\rho} = \text{const.}$$

(N.B. possibly do Gauge transf. on ψ)

$$p_i = p_0 + \rho \left(\frac{\partial \psi_i}{\partial t} + \frac{1}{2} |v_i|^2 \right)$$

no surface tension

$$0 = \frac{(p_1 - p_2)|_{y=h}}{\rho} = \underbrace{\frac{\partial \psi_2}{\partial t} - \frac{\partial \psi_1}{\partial t}}_{\frac{\partial \phi_2}{\partial t} - \frac{\partial \phi_1}{\partial t}} + \frac{1}{2} \underbrace{(|v_1|^2 - |v_2|^2)}_{\approx \frac{1}{2} \omega \left(\frac{\partial \phi_2}{\partial x} + \frac{\partial \phi_1}{\partial x} \right)} \quad (3)$$

Ansatz: $h = H(k) \exp i k x$,
 $\phi_1 \sim h \exp -k y$, $\phi_2 \sim -h \exp +k y$. ($\nabla^2 \phi = 0$)

Ausgabe:

$$h = f(t) \exp ikx$$

$$\phi_1 \sim h \exp -ky$$

$$\phi_2 \sim h \exp +ky.$$

(Motivation $\nabla \cdot v = 0 \Rightarrow \nabla^2 \psi = 0$).

$$(1) + (2): -k(\phi_1 - \phi_2) = 2\dot{h}$$

$$(1) - (2): -k(\phi_1 + \phi_2) = \omega h ik$$

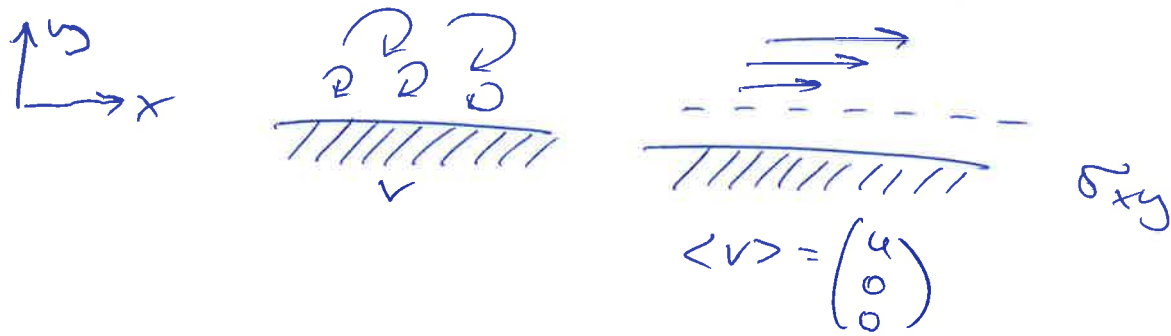
$$(3): \underbrace{\frac{\partial}{\partial t}(\phi_1 - \phi_2)}_{-\frac{2}{k}\dot{h}} = \underbrace{\frac{1}{2}\omega ik(\phi_1 + \phi_2)}_{-\omega h}$$

$$\ddot{h} = \frac{1}{4}(k\omega)^2 h.$$

$$h \sim \exp \pm \frac{k\omega}{2} t.$$

\Rightarrow unstable solution
 \Rightarrow undulations of vortex sheet grow.

The logarithmic velocity profile $u \propto \ln y$



• $\sigma_{xy} : \frac{N}{m^2} = \frac{kg \cdot m/s}{s \cdot m^2} = \text{momentum flux.}$

$$v^* = \sqrt{\sigma_{xy} / \rho}$$

• $u = u(y)$

$$\frac{\partial u}{\partial y} = f(\sigma, \rho, y) = \frac{1}{\chi} \frac{v^*}{y}, \quad \chi = 0.4.$$

$$u = \frac{v^*}{\chi} \ln(y/c)$$

What is c ?

• Viscous boundary layer.

$$Re = \rho \frac{v^* y_0}{\mu}$$

$$Re \sim 1 \Rightarrow y_0 \sim \frac{\mu}{\rho v^*}$$

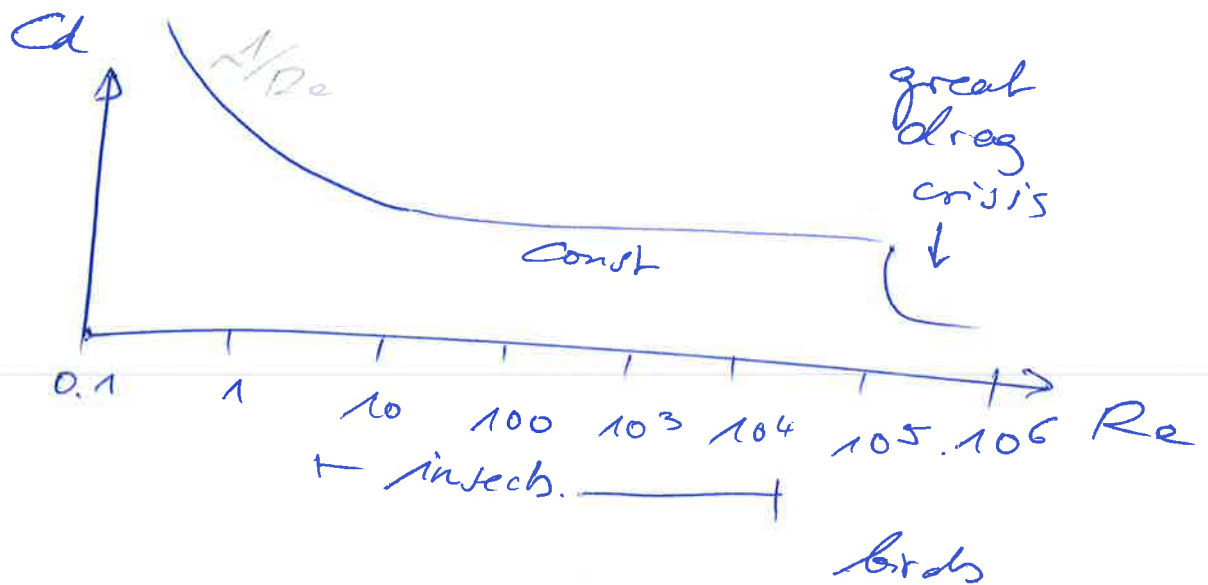
$$y \ll y_0: u = \frac{\sigma}{\chi} y = \frac{\rho v_*^2}{\chi} y \Rightarrow u \sim v_* \ln(y/y_0)$$

• Matching near and far-field

$$u = \frac{v^*}{\chi} \ln\left(\frac{y}{y_0}\right) \equiv \text{log. velocity profile}$$

Drag coefficients and the Reynolds number.

$$F_{\text{drag}} = \left(\frac{1}{2} \rho A u^2 \right) \cdot C_d(Re)$$

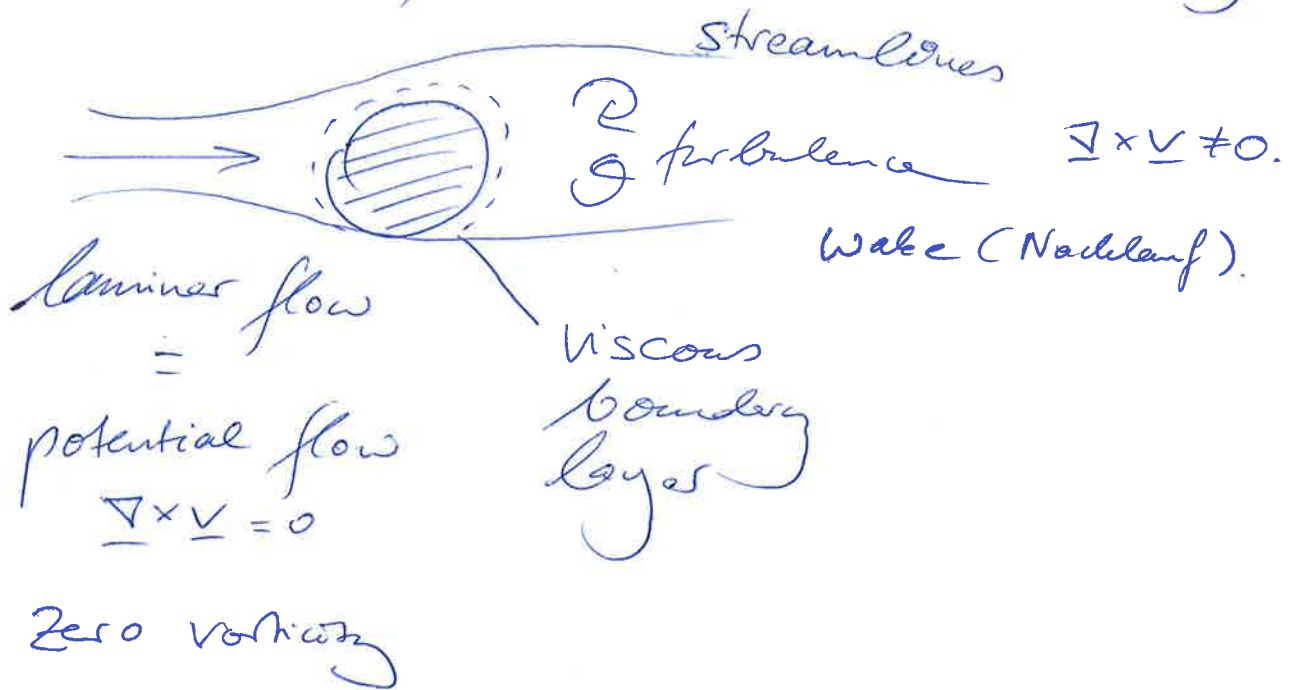


skin friction dominates.

pressure drag:
fluid accelerated to flow around body; drag due to volume - but dissipated at surface

for bodies in inviscid boundary layers. Separation point moves forward.

Turbulent flow around a body



$$F = \text{const. } \rho \cdot u^2 \cdot L^2 \quad \text{Re} \gg 1.$$

$$= \text{const. } \gamma \cdot u \cdot L \quad \text{Re} \ll 1.$$

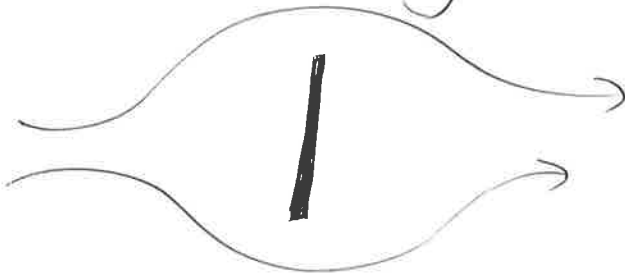
Two Contributions to Hydrodynamic drag at high Re .

- skin friction



Energy dissipation in viscous boundary layers.
→ wetted area important.

- pressure drag.



- at $Re=0$:

flow antisymmetric w/ front / back - reflection

- at high Re :

difference in kinetic pressure $\frac{\rho v^2}{2}$ between front and back.

front

↓
Energy invested to accelerate fluid

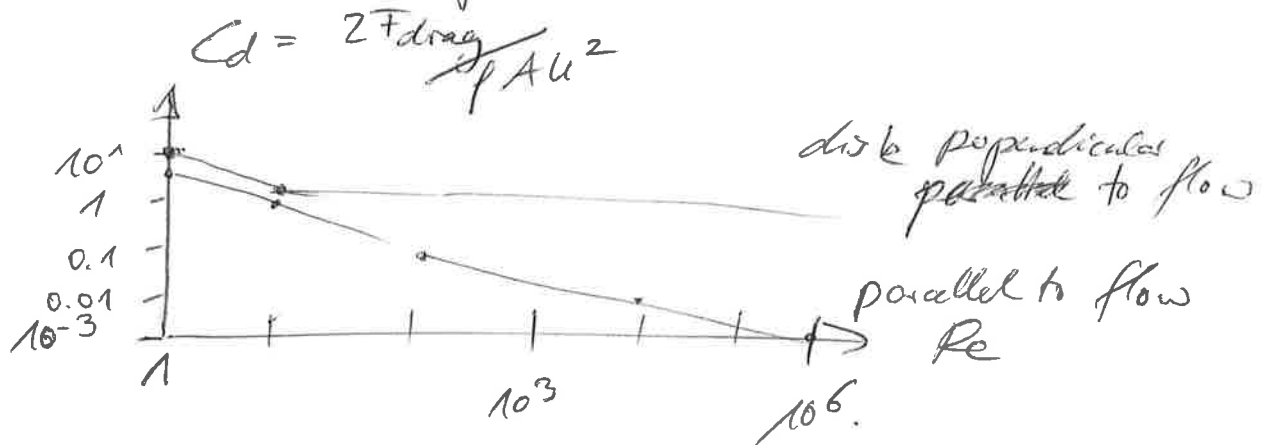
back

↓
Kinetic energy dissipated due to viscosity



Cross-sectional area important.

Experimental example.

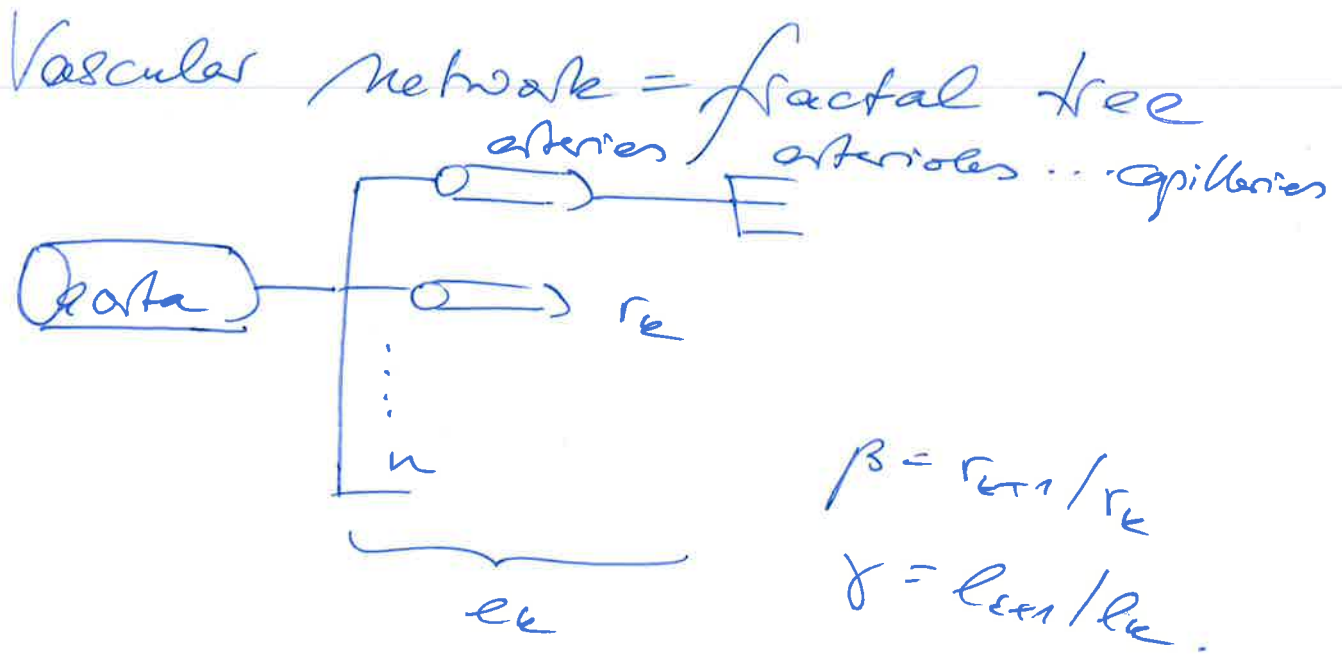


- disk-perpendicular to flow:
pressure drag dominates.
- disk parallel to flow.
skin friction dominates.
 $F_d \sim U \Rightarrow C_d \sim \frac{1}{Re}$.

West et. al.:
Metabolic Scaling.

$$\text{Metabolism } B \sim M^{3/4}$$

N.B. ongoing controversy.



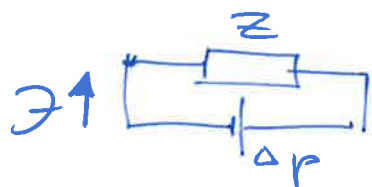
$$N_c = n^N = 10^{10} \text{ for humans.}$$

Metabolism

$$\begin{aligned} B &\sim \text{blood flow} \neq \frac{A \Delta p}{\eta L} \tau_0 \\ &= N_c \tau_0 \\ &= N_c \bar{u} r_c^2 \bar{u}_c \\ &\sim N_c = aN \equiv \text{total number} \\ &\quad \text{of capillaries} \end{aligned}$$

Blood pressure

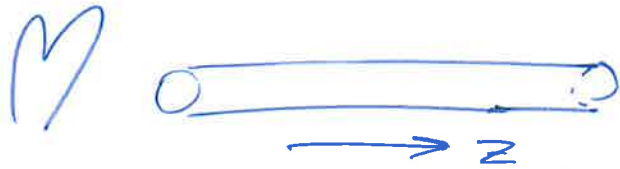
$$\Delta p = \tau_0 \cdot Z. \quad (\text{electric analogy})$$



Cardiac output

$$W = \tau_0 \cdot \Delta p.$$

$$\rho \frac{\partial v}{\partial t} = -\nabla p + \gamma \nabla^2 v \quad (*)$$



$$\frac{\partial p}{\partial z} = p_0 \exp i\omega_0 t$$

Ansatz $\underline{v} = u(r) \exp i\omega_0 t \underline{e}_z$.

(*) gives:

$$\rho i\omega_0 u = -p_0 + \gamma \left(u_{rr} + \frac{1}{r} u_r \right)$$

Laplace op. polar coordinates

→

$$u(r) = \frac{i p_0}{\rho \omega_0} \left(1 - \frac{\mathcal{E}_0(i^{3/2} \alpha (1/R))}{\mathcal{E}_0(i^{3/2} \alpha)} \right)$$

$$\alpha = \sqrt{\frac{\omega_0 \rho}{\gamma}} R \equiv \text{Womersley number}$$

$$\text{flux} = 2\pi \int_0^R u(r) r dr$$

= 15 arteries
 5 arterioles
 0.05 capillaries
 0.005 capillaries

$$\frac{-i\sqrt{\pi} p_0 R^4}{\gamma} \frac{\exp i\omega_0 t}{\alpha^2} \frac{\mathcal{E}_2(i^{3/2} \alpha)}{\mathcal{E}_0(i^{3/2} \alpha)}$$

$$= \begin{cases} \frac{\sqrt{\pi} p_0 R^4}{8\gamma} & |\alpha| \ll 1 \\ \frac{\sqrt{\pi} p_0 R^2}{\omega_0 \rho} & |\alpha| \gg 1 \end{cases}$$

impedance = $Z = \frac{\Delta p}{\text{flux}}$, $\Delta p = l \cdot \frac{\partial p}{\partial z}$.

$$|Z| = \frac{8 \eta l}{\pi R^4}$$

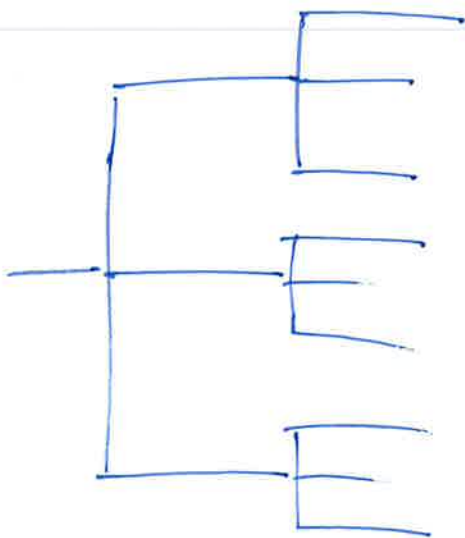
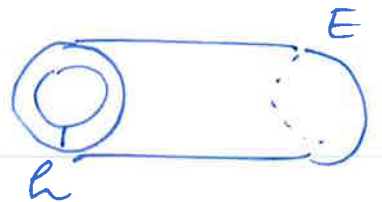
$$|\alpha| \ll 1$$

\equiv Poiseuille flow

$$|Z| = \frac{f W_0 l}{\pi R^2}$$

$$|\alpha| \gg 1$$

N.B. elasticity of vessel walls gives correction



$$|Z| = \frac{\rho C_0}{\pi R^2}$$

$$C_0 = \sqrt{\frac{E h}{2 \rho R}}$$

aorta
 $\alpha = 15$

arteries
 $\alpha = 5$

arterioles
 $\alpha = 0.05$

capillaries
 $\alpha = 0.005$

inertial effects dominate

pulsatile flow

viscous effects dominate

non-pulsatile flow

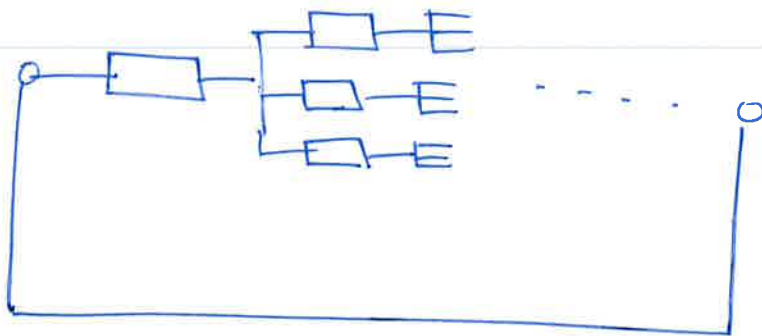
Non-pulsatile flow.

viscous resistance (impedance)

$$R_k = \frac{8 \eta l_k}{\pi r_k^4}$$

Resistance of network.

$$Z = \sum_{k=0}^N \frac{R_k}{N_k} \approx \frac{R_c}{N_c}$$

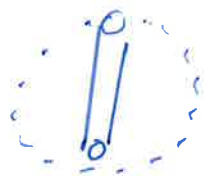


(electrical analogy)

The concept of
price volumes:

$$V_{tot} = \frac{4}{3} \pi \cdot \left(\frac{l_t}{2}\right)^3 N_k$$

$k=0$



$k=1$



...

$$\Rightarrow \gamma^3 = \frac{l_{k+1}^3}{l_k^3} = \frac{N_k}{N_{k+1}} = \frac{1}{n}$$

$$\boxed{\gamma \sim n^{-1/3}}$$

Impedance Matching

- Non-pulsatile flow

$$R_k = \frac{1}{n} R_{k+1}$$

$$\Rightarrow \frac{l_k}{r_k^4} = \frac{1}{n} \frac{l_{k+1}}{r_{k+1}^4}$$

$$\Rightarrow \beta^4 = 1/n \Rightarrow \beta = n^{-1/4}$$

Murray's law: $n \beta^3 = \text{const. across levels}$

- pulsatile flow

$$R_k = \frac{1}{n} R_{k+1}$$

$$\frac{1}{r_k^2} = \frac{1}{n} \frac{1}{r_{k+1}^2}$$

$$\Rightarrow \beta = n^{-1/2}$$



pulsatile
- number of levels changes with n .

non-pulsatile
- number of levels constant

$$\alpha = \frac{1}{n \gamma \beta^2} \sim n^{1/3}$$

$$M \sim V_{\text{blood}} \sim N_{\text{tot}} \sqrt{n} r_c^2 l_c (1 + \alpha^2 + \alpha^4 + \dots + \alpha^{2N})$$
$$\sim N_{\text{tot}}^{4/3}$$

$$B \sim N_{\text{tot}}$$

\Rightarrow

$$B \sim M^{3/4}$$

N.B.

refinement: l_c not constant

$$N_{\text{tot}} l_c^3 = N_{\text{tot}}^{4/3} l_c$$
$$\rightarrow l_c \sim N_{\text{tot}}^{1/6}$$

.....